

Robust Real-Time Segmentation of Images and Videos Using a Smooth-Spline Snake-based algorithm

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Abstract—This paper deals with fast image and video segmentation using active contours. Region-based active contours using level sets are powerful techniques for video segmentation, but they suffer from large computational cost. A parametric active contour method based on B-Spline interpolation has been proposed in [26] to highly reduce the computational cost, but this method is sensitive to noise. Here, we choose to relax the rigid interpolation constraint in order to robustify our method in the presence of noise: by using smoothing splines, we trade a tunable amount of interpolation error for a smoother spline curve. We show by experiments on natural sequences that this new flexibility yields segmentation results of higher quality at no additional computational cost. Hence, real-time processing for moving objects segmentation is preserved.

I. INTRODUCTION

WE address the problem of image and video segmentation using region-based active contours. The goal is to extract image regions corresponding to semantic objects. Image and video segmentation can be cast in a minimization framework by choosing a criterion which includes region and boundary functionals. Boundary functionals were first proposed by Kass *et al.* [21] and geodesic active contours by Caselles *et al.* [3], [4] for active contour segmentation. Region-based active contours were first introduced by Ronfard *et al.* [30] and Cohen *et al.* [10]. Chakraborty *et al.* [5] combined both boundary and region information for medical images segmentation. Then, Chesnaud *et al.* [9], Chan *et al.* [6], Zhu *et al.* [35], Paragios *et al.* [24], and Debreuve *et al.* [12] introduce region-based statistic descriptors for image or video segmentation. Jehan-Besson *et al.* [17], [20] address the segmentation problem where features of the region to be segmented are embedded in region functionals. In this framework, Gastaud *et al.* [13] propose a new approach introducing shape prior. This method uses a variational approach as opposed to previous work on shape prior, based on probabilistic methods [11]. The shape prior allows free form deformation [13] and is not restricted to a parametric deformation as in [8].

All these contour or region-based methods use a level-set approach which is accurate but time consuming. In this paper, we

propose a parametric active contour evolution based on a cubic spline contour [2].

In Section II, we present a survey of the region-based criterion, the derivation of the criterion and computation of the velocity vector.

In Section III, we propose a cubic B-spline implementation. Cubic B-splines preserve C^2 regularity and have excellent approximation properties [32] which means that, for a given accuracy, fewer samples are needed than with other parametric methods; moreover, fast algorithms are available for B-splines, which greatly reduces the computation cost.

Unfortunately, interpolation methods are not robust to noise. This is why we propose to use smoothing splines [33] in the B-spline interpolation approach of [27]. These curves preserve the implementation advantages as the B-splines while softening the interpolation constraint. The relaxation of the interpolation condition is traded for an *optimal* increase of the smoothness of the spline snake. A smoothness parameter controls the amount of relaxation.

In Section IV, we compare the influence of the smoothing spline parameter with the curve-length regularization coefficient. Finally, we show some experiments on real video sequences.

II. REGION-BASED ACTIVE CONTOURS

A. Criterion and Velocity

Let us define a general segmentation criterion. For each frame of the sequence, we search a background region Ω_{out} , and object regions Ω_{in} with a common boundary Γ (Fig. 1). Thus, the criterion includes both region and boundary functionals

$$J(\Omega_{\text{out}}, \Omega_{\text{in}}, \Gamma) = \underbrace{\int_{\Omega_{\text{out}}} k_{\text{out}}(\Omega_{\text{out}}) d\sigma + \int_{\Omega_{\text{in}}} k_{\text{in}}(\Omega_{\text{in}}) d\sigma}_{\text{Region terms}} + \underbrace{\int_{\Gamma} \beta ds}_{\text{Boundary term}} \quad (1)$$

In this criterion, k_{out} is the descriptor of the unknown background domain Ω_{out} , k_{in} is the descriptor of the unknown object domain Ω_{in} and β is the weight of the regularization.

Since we use statistical descriptors (for k_{in} and k_{out}), such as mean, variance, or region histograms, the entropy descriptors are globally attached to the region Ω [9]. In the variational

Manuscript received October 6, 2003; revised May 10, 2004. The associate editor coordinating the review of this manuscript and approving it for publication was Dr. Nicolas Merlet.

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Digital Object Identifier 10.1109/TIP.2005.849307

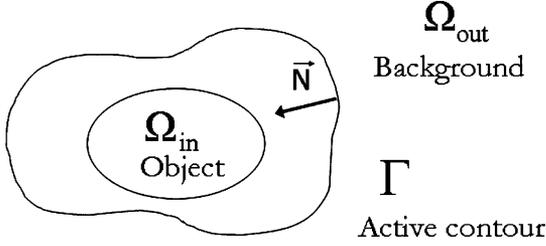


Fig. 1. Domain definition.

Eulerian method proposed by Jehan-Besson *et al.* [20], for a region-based active contour segmentation, the authors introduce a dynamical scheme (shape gradient method) in the criterion. Hence, regions become continuously dependent on an evolution parameter τ .

The criterion $J(\Omega_{\text{out}}(\tau), \Omega_{\text{in}}(\tau), \Gamma(\tau))$ is denoted by $J(\tau)$. Thus, the computation of the derivative provides

$$\begin{aligned}
 J'(\tau) = & \underbrace{\int_{\Omega_{\text{out}}(\tau)} \frac{\partial k_{\text{out}}}{\partial \tau} d\sigma + \int_{\Omega_{\text{in}}(\tau)} \frac{\partial k_{\text{in}}}{\partial \tau} d\sigma}_{(a)} \\
 & + \underbrace{\int_{\Gamma(\tau)} (k_{\text{out}} - k_{\text{in}})(\mathbf{v} \cdot \mathbf{N}) ds}_{(b)} \\
 & + \underbrace{\int_{\Gamma(\tau)} (-\beta \cdot \kappa + \nabla \beta \cdot \mathbf{N})(\mathbf{v} \cdot \mathbf{N}) ds}_{(c)} \quad (2)
 \end{aligned}$$

where κ is the curvature of the contour, \mathbf{v} is the velocity of $\Gamma(\tau)$, and \mathbf{N} is the unit inward normal to $\Gamma(\tau)$.

The terms (a) are deduced from the variation of the descriptors with the region. The term (b) is deduced from the variation of the region, and the classical term (c) comes from the derivation of the Boundary term in (1) [4]. Complete proofs are available in [17], [19], and [20].

The active contour $\Gamma(\tau)$ evolves from an initial position $\Gamma(0)$ toward the object with a velocity \mathbf{v} in the direction of \mathbf{N} , the inward normal vector of the active contour

$$\begin{cases} \frac{\partial \Gamma(\tau)}{\partial \tau} = \mathbf{v} \mathbf{N} \\ \Gamma(0) = \Gamma_0. \end{cases} \quad (3)$$

The velocity expression is deduced from the derivative (2)

$$\mathbf{v} = \mathbf{A} + k_{\text{in}} - k_{\text{out}} + \beta \kappa. \quad (4)$$

- \mathbf{A} represents local terms which are computed from the two first terms (a) in (2). In Section IV, we will detail the expression of \mathbf{A} and then the velocity \mathbf{v} for two applications: segmentation of homogenous regions and segmentation of moving objects.
- β is a constant.

B. Implementation

Region-based active contour evolution can be implemented in two different ways.

- *Implicitly*, based on the level-set approach [19], [20], [23]. Such a method provides an implicit management of topological changes and yields accurate results, but it suffers from a high computational cost.
- *Explicitly*, using active parametric contours. Such a method reduces the computational cost substantially and provides a complete control of the data size. The accuracy of the results is dependent on the noise level of the sequence. Using smoothing splines is likely to introduce robustness in this method.

III. TOWARDS CUBIC SMOOTHING SPLINES

A. Cubic Spline Interpolation

The evolution velocity is now computed only at sampling points along a spline active contour. Cubic spline curves are parametric curves $S(t) = (x(t), y(t))$ where $x(t)$ and $y(t)$ are cubic polynomials on each segment $t_k \leq t \leq t_{k+1}$ and are smoothly (twice continuously differentiable) connected between segments. Here, we assume that there are n such segments parametered by t_0, t_1, \dots, t_{n-1} with the assumption $t_n = t_0$ and that we are given the n sampling points $P_k = S(t_k)$.

Each segment $t_k \leq t \leq t_{k+1}$ is expressed as a cubic polynomial [1]

$$\begin{aligned}
 S(t) = & Q_{k-1} B_{k-3}^3(t) + Q_k B_{k-2}^3(t) \\
 & + Q_{k+1} B_{k-1}^3(t) + Q_{k+2} B_k^3(t). \quad (5)
 \end{aligned}$$

$B_k^3(t)$ is a nonuniform B-spline function; the n parameters of the model are the B-spline coefficients Q_k called *control points*. These coefficients can be specified by solving for Q_k the n equations $S(t_k) = P_k$.

The B-spline function $B_k^3(t)$ is a piecewise cubic polynomial that depends on the n values t_k of the curve parameter at the sampling points.

Irregular sampling of t is intuitively more pertinent, as regards active contour propagation, than uniform sampling. This is the option chosen by, e.g., Pottmann *et al.* [25] and Yang *et al.* [34], who propose to optimize the parameterization of the spline curve for approximating a target curve, as well as in other approaches based on arbitrary parameterizations (chord length, centripetal, Foley, etc.). However, building the nonuniform spline curve requires the computation of n different polynomials B_k^3 which is time consuming. To overcome this problem, we have proposed a regular sampling approach [27], i.e., $t_k = k$, to represent the active contour using uniform B-spline functions. In that case, after reparameterizing the curve, the B-spline function $B_k^3(t)$ is independent of the segment considered on the curve. We can write $B_k^3(t) = \beta^3(t - k)$ where the centered B-spline of degree 3 $\beta^3(t)$ is a bell-shaped, symmetrical function, as shown in Fig. 2, defined by

$$\beta^3(t) = \begin{cases} \frac{2}{3} - |t|^2 + \frac{|t|^3}{2}, & 0 \leq |t| < 1 \\ \frac{(2-|t|)^3}{6}, & 1 \leq |t| < 2 \\ 0, & 2 \leq |t|. \end{cases} \quad (6)$$

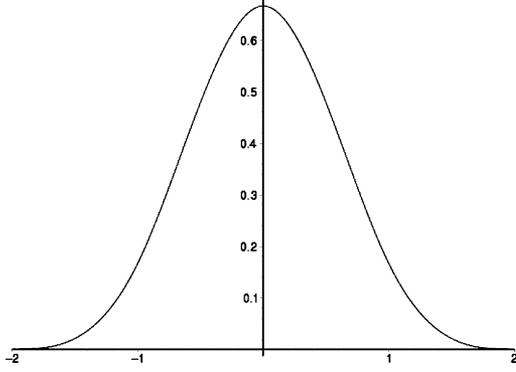


Fig. 2. Centered B-spline of degree 3.

The arc (5) with (6) becomes [1]

$$\begin{aligned}
 S(t) = & \left(-\frac{1}{6}Q_{k-1} + \frac{1}{2}Q_k - \frac{1}{2}Q_{k+1} + \frac{1}{6}Q_{k+2} \right) t^3 \\
 & + \left(\frac{1}{2}Q_{k-1} - Q_k + \frac{1}{2}Q_{k+1} \right) t^2 \\
 & + \left(-\frac{1}{2}Q_{k-1} + \frac{1}{2}Q_{k+1} \right) t \\
 & + \frac{1}{6}Q_{k-1} + \frac{2}{3}Q_k + \frac{1}{6}Q_{k+1} \text{ for } t \in [k, k+1]. \quad (7)
 \end{aligned}$$

The computation cost of regular sampling is lower than handling a specific equation for each segment $t_k \leq t \leq t_{k+1}$ of a nonuniform B-Spline curve.

Moreover, the control points Q_k can be obtained from the sampling points P_k using a fast filtering algorithm when the curve parameter is sampled uniformly (see Appendix I).

Indeed, each interpolated point P_k corresponds to the polynomial expression value $S(t)$ when $t = k$. From (7), we obtain the relation between sampling points P_k and control points (B-spline coefficients) Q_k

$$S(k) = P_k = \frac{1}{6}(Q_{k-1} + 4Q_k + Q_{k+1}). \quad (8)$$

This relation can be written as a convolution

$$Q_k = (B_1^3)^{-1} * P_k \quad (9)$$

where B_1^3 is the discrete cubic B-spline kernel.

The inverse convolution operator is defined by

$$B_1^3(z)^{-1} = \frac{6}{z + 4 + z^{-1}}. \quad (10)$$

Using the prefiltering approach exposed in [33], the inverse convolution operator $(B_1^3)^{-1}$ is computed efficiently from a cascade of first order causal and anti-causal recursive filters (see details in Appendix I). The control points Q_k are computed from sampling points P_k using this fast filtering algorithm.

Cubic splines provide good interpolation accuracy at low computational cost [32]. Moreover, these curves have several interesting properties: They are twice continuously differentiable, which allows to build a C^2 -regular curve. Thus, the normal vector and the curvature, involved in the velocity

equation, can be computed exactly at every sampling point. In addition, such curves minimize the following criterion:

$$\int_{\Gamma} \|C''(t)\|^2 dt \quad (11)$$

under interpolatory constraints [31]. Here, $C(t) = (x(t), y(t))$ is a parametric description of the curve Γ and $C''(t)$ the second derivative of $C(t)$ w.r.t. t ; this functional is actually very close to the (squared) curvature κ^2 when the parameter t is close to the curvilinear abscissa, as shown in [16].

Although we have obtained real-time accurate results with an implementation based on these B-spline curves [26], interpolation is not robust enough in the presence of noise. Thus, we propose to use a less constrained approximation method; namely, the smoothing spline method [28].

B. Cubic Spline Approximation

A smoothing spline is an approximation curve controlled by a parameter trading interpolation error for smoothness [29]. It minimizes the following criterion:

$$\int_{\Gamma} \|C''(t)\|^2 dt + \frac{1}{\lambda} \sum (P_k - C_k)^2 \quad (12)$$

where the P_k s are the measured data points and C_k s are points, on the curve, joining of polynomial pieces.

The result is still a cubic spline, but it does not satisfy anymore the interpolation condition exactly. The interpolation error has been converted into increased smoothness—smaller energy of the second derivative.

The first term of (12) can be developed as

$$\begin{aligned}
 \|C''\|^2 &= \frac{|x'x'' + y'y''|^2}{x'^2 + y'^2} + \frac{|x'y'' - x''y'|^2}{x'^2 + y'^2} \\
 &= \left| \frac{d}{dt} \sqrt{x'^2 + y'^2} \right|^2 + (x'^2 + y'^2) \left| \frac{d}{dt} \arctan \left(\frac{y'}{x'} \right) \right|^2 \\
 &= s'^2 + s'^2 \phi'^2
 \end{aligned}$$

where s is the curvilinear abscissa of the curve Γ , and $\phi(t)$ is the angle of the tangent to the curve at $C(t)$. This shows that the smoothing part in (12) can be rewritten as a sum of two positive terms

$$\int_{\Gamma} \|C''(t)\|^2 dt = \int_{\Gamma} s'^2(t) dt + \int_{\Gamma} s'^2(t) \phi'^2(t) dt. \quad (13)$$

Thus, the decrease of $\int_{\Gamma} \|C''(t)\|^2 dt$ facilitates the decrease of $\int_{\Gamma} s'^2(t) dt$ and $\int_{\Gamma} s'^2(t) \phi'^2(t) dt$:

- the first term of (13) represents the average variation of curvilinear abscissa. Thus, decreasing this term tends to improve the curve sampling uniformity;
- when the sampling is nearly uniform—i.e., $s'(t) \approx \text{Constant}$, which is favored by the decrease of the first term—the second term of (13) is lower bounded by the square of (using Cauchy–Schwartz inequality)

$$\frac{\text{length}(\Gamma)}{(\# \text{ control points})^{3/2}} \int_{\Gamma} |\phi'(t)| dt$$

which is the average tangent angle variation over the curve. Preventing this quantity from being large also

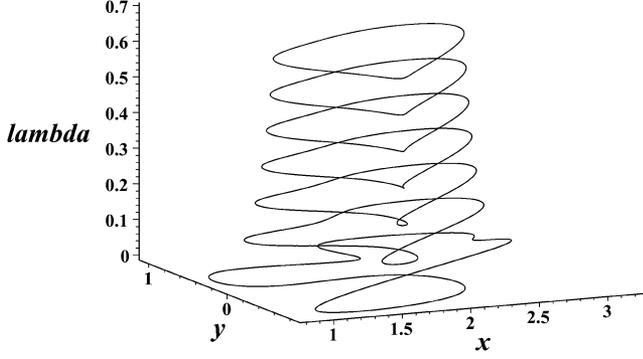


Fig. 3. Evolution from cubic spline interpolation ($\lambda = 0$) toward cubic smoothing spline approximation ($\lambda = 0.7$).

prevents loops in the curves. This is because each loop increases the value of $\int_{\Gamma} |\phi'(t)| dt$ by π at least.

Fig. 3 shows the evolution of a cubic spline curve, based on 10 data points, from regular interpolation (for $\lambda = 0$) toward a smoothing spline approximation (for $\lambda = 0.7$). This figure shows that loops are avoided as the smoothness parameter λ increases.

In Figs. 4 and 5, we have plotted the variance of the curvilinear abscissa $\int_{\Gamma} s''(t)^2 dt$ and the interpolation error of smoothing splines as functions of the smoothness parameter λ .

The curve in Fig. 4 confirms that the interpolation error increases *slightly* with λ . Indeed, the amount of missclassified pixels, between the smoothing spline segmentation and a segmentation of reference, increases with λ , but only up to 1.6% of the size of the object.

Fig. 5 shows that, on the contrary, the curvilinear abscissa variance decreases with λ .

The relation between sampling points P_k and control points Q_k (B-spline coefficients) can be written as a convolution

$$Q_k = (S_{\lambda}^3)^{-1} * P_k \quad (14)$$

with

$$S_{\lambda}^3(z)^{-1} = \frac{6}{z + 4 + z^{-1} + 6\lambda(z^{-2} - 4z^{-1} + 6 - 4z + z^2)}. \quad (15)$$

This transfer function is factorized into a product of causal and anticausal responses

$$\frac{b}{\lambda} \cdot \frac{1}{1 + az^{-1} + bz^{-2}} \cdot \frac{1}{1 + az + bz^2} \quad (16)$$

where $a = -(z_0 + z_1)$ and $b = z_0 z_1$ are real quantities obtained from the two poles z_0 and z_1 of $S_{\lambda}^3(z)^{-1}$ that are *inside* the unit circle. This prefiltering approach provides an efficient method to compute the smoothing spline coefficients (see details in Appendix II).

The positive parameter λ quantifies the tradeoff between interpolation error and regularity. For $\lambda = 0$, no interpolation error is allowed, and, thus, we get interpolating splines. When λ increases, a larger amount of interpolation error is allowed; hence, the spline snake is smoother and its sampling more regular. We show in Section IV the benefits of this new approach for the segmentation of noisy images.

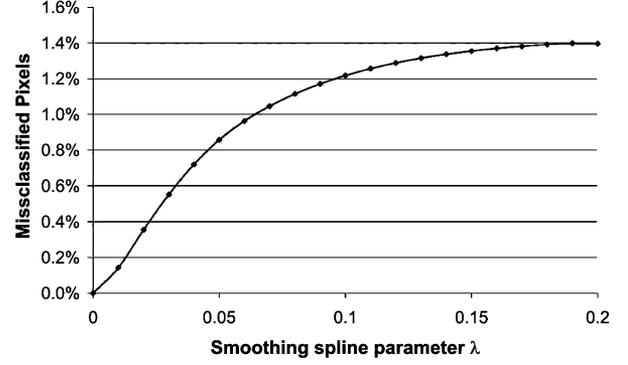


Fig. 4. Accuracy decreases *slightly* with λ .

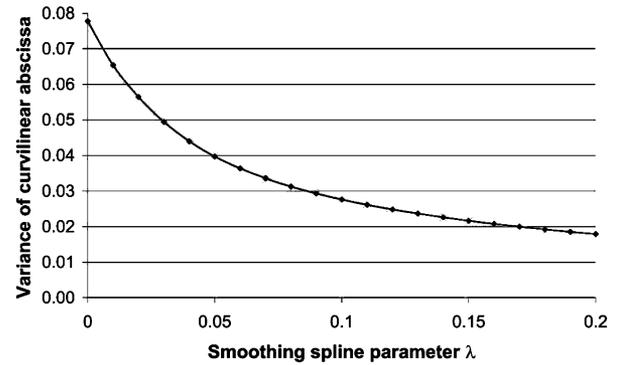


Fig. 5. Sampling uniformity increases with λ .

IV. SEGMENTATION OF NOISY DATA

In this section, we present results of segmentation of static images and segmentation of video sequences. We compare the respective influence of the smoothing spline parameter λ and the contour length regularization parameter β on the segmentation quality. We first show results of a segmentation based on a homogeneity criterion.

A. Segmentation of Homogeneous Regions

1) *Grayscale Still Images*: In this example, the images are osteoporosis medical images. The goal is to segment bone regions in the image. We consider the functional (1) where k_{out} and k_{in} are descriptors of the bone homogeneity. The region homogeneity is characterized by a function of the variance of luminance intensity. Let σ_{out}^2 and μ_{out} represent respectively the variance and mean of $\Omega_{\text{out}}(\tau)$, σ_{in}^2 , and μ_{in} represent, respectively, the variance and mean of $\Omega_{\text{in}}(\tau)$, and $\Phi(r)$ a positive $C^1(\mathbb{R})$ function, for instance, $\Phi(r) = \log(1 + r^2)$.

Thus, the criterion to be minimized is

$$J(\Omega_{\text{out}}, \Omega_{\text{in}}, \Gamma) = \int_{\Omega_{\text{out}}} \Phi(\sigma_{\text{out}}^2) d\sigma + \int_{\Omega_{\text{in}}} \Phi(\sigma_{\text{in}}^2) d\sigma + \int_{\Gamma} \beta ds \quad (17)$$

where β is a positive constant.

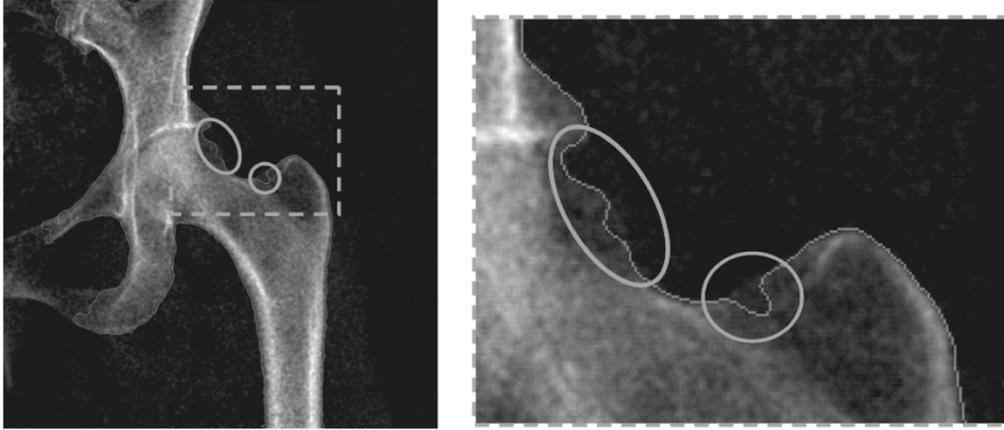


Fig. 6. Regular spline segmentation with $\lambda = 0$ and length penalty $\beta = 10$.

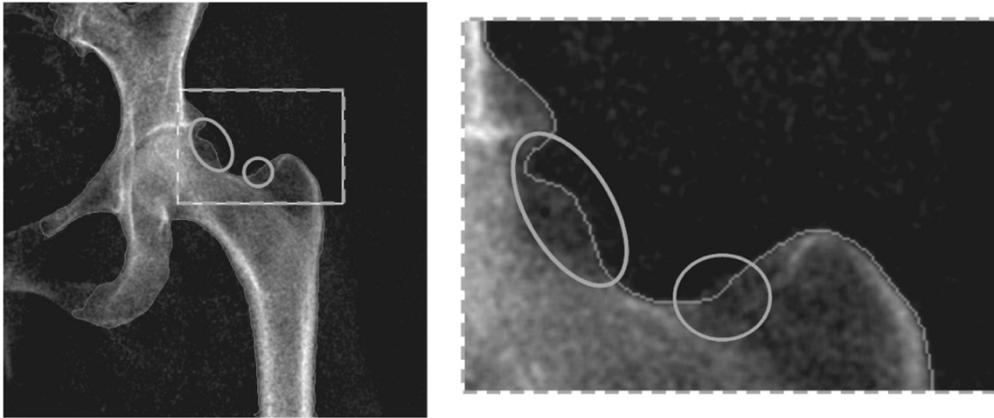


Fig. 7. Smoothing spline segmentation with $\lambda = 0.08$ and $\beta = 0$.

Using (2), the derivative of the functional J with respect to τ is

$$\begin{aligned}
 J'(\tau) = & - \int_{\Gamma(\tau)} \left[\Phi(\sigma_{\text{in}}^2) - \Phi(\sigma_{\text{out}}^2) + \beta\kappa \right. \\
 & + \Phi'(\sigma_{\text{in}}^2) [(I - \mu_{\text{in}})^2 - \sigma_{\text{in}}^2] \\
 & \left. - \Phi'(\sigma_{\text{out}}^2) [(I - \mu_{\text{out}})^2 - \sigma_{\text{out}}^2] \right] \\
 & \cdot (\mathbf{v} \cdot \mathbf{N}) ds
 \end{aligned} \quad (18)$$

where κ is the curvature of the contour and β is a constant.

More details and proofs are available in Jehan-besson *et al.* [19]. In order to find a local extremum of the criterion (17), as the authors proposed, we evolve a curve using the steepest descent method. Thus, we obtain the following evolution equation:

$$\frac{\partial \Gamma(\tau)}{\partial \tau} = \mathbf{v} \cdot \mathbf{N}.$$

Thus, the expression (4) of the velocity \mathbf{v} is known

$$\begin{aligned}
 v = & \Phi(\sigma_{\text{in}}^2) - \Phi(\sigma_{\text{out}}^2) + \beta\kappa \\
 & + \Phi'(\sigma_{\text{in}}^2) [(I - \mu_{\text{in}})^2 - \sigma_{\text{in}}^2] \\
 & - \Phi'(\sigma_{\text{out}}^2) [(I - \mu_{\text{out}})^2 - \sigma_{\text{out}}^2].
 \end{aligned} \quad (19)$$

This velocity makes the B-spline active contour evolve toward the minimum of the energy criterion (17). Thus, the competition between the region inside the contour $\Omega_{\text{in}}(\tau)$ and the region outside $\Omega_{\text{out}}(\tau)$ leads to increase the homogeneity of both regions. However, the images are corrupted by acquisition noise and by the noise of nonbone tissues (muscles, fat, etc.).

Fig. 6 shows the convergence using the cubic spline interpolation with length penalty method. The length penalty provides smoothness to the contour. However, the acquisition noise corrupts the segmentation quality in the area of interest for osteoporosis diagnostic. The smoothness of the contour depends only on the length penalty parameter β .

Fig. 7 shows the convergence using the new smoothing spline method. The flexibility of the smoothing splines provides an accurate bone segmentation without being corrupted by the noise. The smoothness of the contour depends only on the smoothing spline parameter λ .

Fig. 8 shows the robustness of the new smoothing spline method regarding λ parameter variations. Between the left and the right picture on the top row, λ is only increased from 0 to 0.01 [Fig. 8(a) and (b)], but still the accuracy of the segmentation is highly improved and the most efficient results are almost reached. If we increase again λ ten times, up to 0.1, [Fig. 8(c)], the segmentation is smooth but still very good. By increasing λ ten times [Fig. 8(d)], the contour is too smooth but remains robust. Additional experiments with $\lambda = 10$ and 100 indicate

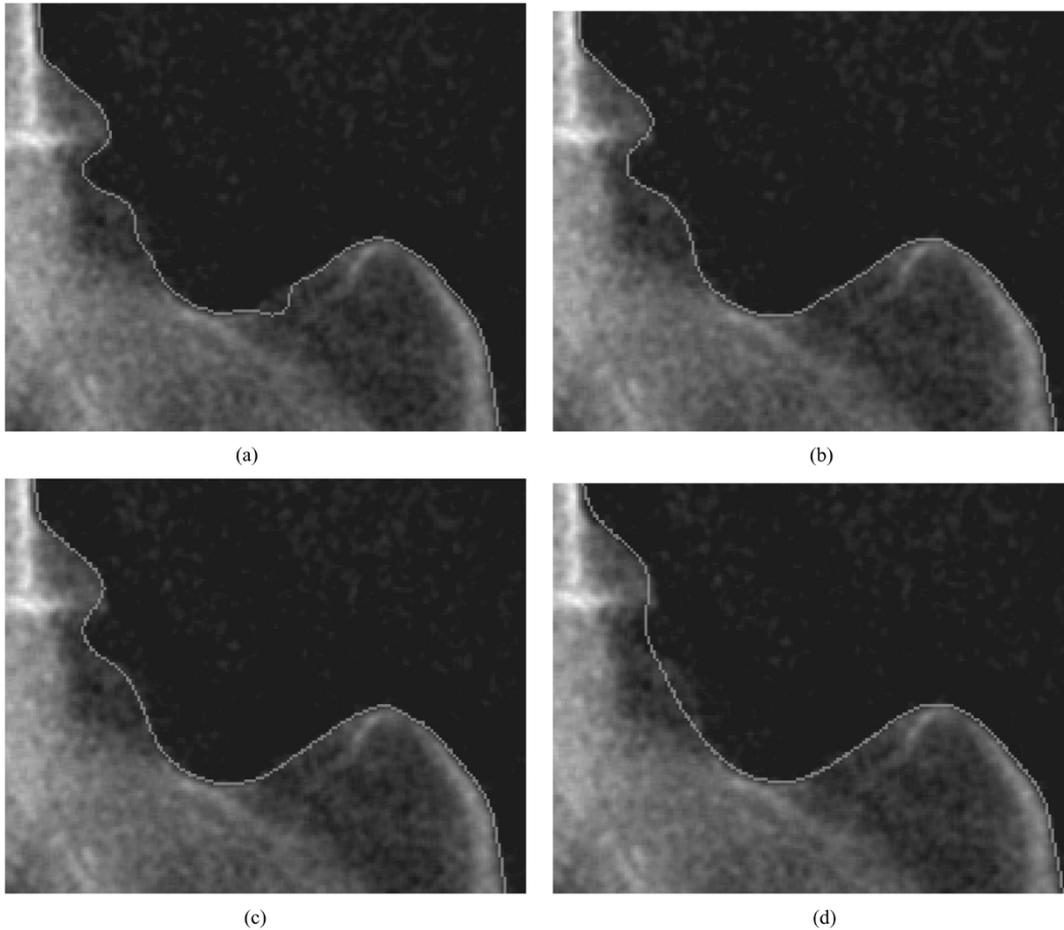


Fig. 8. Robustness regarding Smoothing spline parameter λ variations. (a) Interpolation $\lambda = 0$ and $\beta = 0$. (b) Approximation $\lambda = 0.01$ and $\beta = 0$. (c) Approximation $\lambda = 0.1$ and $\beta = 0$. (d) Approximation $\lambda = 1$ and $\beta = 0$.

that even if the contour is too smooth to preserve a sufficient segmentation accuracy, the structure of the contour remains stable which is not true with variations of β , the weight on the length penalty. Such relative robustness of the snake with respect to λ suggests that we can determine a range for standard values of this parameter. This first experiment provides a range of $[0.1, 1]$.

The contour is sampled with 512 knots and the size of the image is 512×512 . The segmentation is obtained in 25 s with a Pentium IV at 2.6 GHz. It has to be pointed out that most of this computation time is spent in evaluating the variance of the object domain and of the background. Indeed, segmentations with 256 and 128 knots, obtained in 24 s, confirm it: The cost of the approximation amounts to a few percents of the full computation.

To improve the computation time of our algorithm with such descriptors based on area moments (mean of the intensity, variance, etc.), a perspective would be to implement the method of Jacob *et al.* [15] for an exact computation of the area moments of spline curves.

2) *Color Video Sequences*: As detailed by Jehan *et al.* in [19], [20], the homogeneity in color images is related to the determinant of the covariance matrix for Gaussian distributions.

Yezzi *et al.* [22] and Herbulot *et al.* [14] extended this framework to the more general case of Entropy descriptors without Gaussian distribution hypothesis.

In these experiments, regions of interest are regions of homogeneous color, like the face on the sequence *Erik*. The color images are in the RGB color space. Let us define the joint probability distribution

$$q(I_R(x), I_G(x), I_B(x), x \in \Omega)$$

and the joint entropy, between the three channels of the image, on the domain Ω

$$H_{\text{RGB}}(\Omega) = - \int_{\Omega} q(I_R(x), I_G(x), I_B(x), x \in \Omega) \times \ln q(I_R(x), I_G(x), I_B(x), x \in \Omega) dx. \quad (20)$$

The segmentation of homogeneous regions of a color video sequence is achieved by region competition between the background Ω_{out} and the object Ω_{in} , minimizing the following criterion:

$$J(\Omega_{\text{in}}, \Omega_{\text{out}}, \Gamma) = H_{\text{RGB}}(\Omega_{\text{in}}) + H_{\text{RGB}}(\Omega_{\text{out}}) + \int_{\Gamma} \beta ds. \quad (21)$$



Fig. 9. Evolution of segmentation with the minimization of the criterion (21). (a) Initial curve. (b) Iteration 40. (c) Iteration 100. (d) Final segmentation (Iteration 430).

Thus, applying DREAMS method [20] to (21), the evolution equation based on the joint probability distributions is [14]

$$\begin{aligned} \frac{\partial \Gamma}{\partial \tau}(\tilde{x}) = & \left[-q(I_R(\tilde{x}), I_G(\tilde{x}), I_B(\tilde{x}), \Omega) \right. \\ & \times (\ln q(I_R(\tilde{x}), I_G(\tilde{x}), I_B(\tilde{x}), \Omega) + 1) - \frac{1}{|\Omega|} \\ & \times \left(H_{\text{RGB}}(\Omega) - 1 + \int_{\Omega} K(I_R(x) - I_R(\tilde{x}), \right. \\ & \quad \left. I_G(x) - I_G(\tilde{x}), I_B(x) - I_B(\tilde{x})) \right. \\ & \left. \times \ln q(I_R(x), I_G(x), I_B(x), \Omega) dx \right) \Big] \mathbf{N} \end{aligned} \quad (22)$$

where

$$K(x, y, z) = \frac{1}{2\pi\sigma^2} \exp -\frac{x^2 + y^2 + z^2}{2\sigma^2} \quad (23)$$

is the Gaussian kernel involved in the Parsen window method.

Fig. 9 shows the evolution of the curve and Fig. 10 the segmentation of some frames of a sequence.

The data extracted from the histogram evolution are very sensitive to noise. This is why we use a smoothing B-spline approach which combines a very low computational cost and a

global robustness to noisy data. The parameter $\lambda = 0.1$ is in the standard range determined in the previous experiment, i.e., $[0.1, 1]$.

B. Moving Objects Segmentation

Now, we present results obtained for the segmentation of moving objects in video sequences. This segmentation is based on motion detection. Our method is applied to the real “coast-guard” video. The goal is to detect the boat of the coastguards in the sequence. We consider the functional (1) where k_{in} and k_{out} are, respectively, descriptor of moving objects and descriptor of the background. The descriptors have to take into account the camera motion in this sequence. Thus, the criterion to be minimized is

$$\begin{aligned} J(\Omega_{\text{out}}, \Omega_{\text{in}}, \Gamma) = & \int_{\Omega_{\text{out}}} |I_n(\sigma) - \text{Proj}(I_{n-1}(\sigma))| d\sigma \\ & + \int_{\Omega_{\text{in}}} \alpha d\sigma + \int_{\Gamma} \beta ds \end{aligned} \quad (24)$$

where $\text{Proj}(I_{n-1}(\sigma))$ is the projection of the image I_{n-1} onto the referential of image I_n in order to compensate for the motion of the camera. The camera motion model is based on a 6-parameter affine model. These parameters are computed with a robust



Fig. 10. Segmentation through a sequence. (a) Frame 10. (b) Frame 20. (c) Frame 30. (d) Frame 40.

estimation using motion vectors [7]. The motion field is evaluated by a classical block-matching algorithm between frames I_n and I_{n-1} [18]. β and α are two positive constants.

The descriptors are region-independent. Thus, the local terms of the differentiation (2) disappear and the velocity (4) reduces to

$$v = k_{\text{in}} - k_{\text{out}} + \beta\kappa. \quad (25)$$

Since the descriptor $k_{\text{out}} = |I_n - \text{Proj}(I_{n-1})|$ is a temporal gradient, this local term is noise sensitive.

In the “coastguard” sequence Fig. 11(a), the wake of the boat behaves like noise for the background descriptor k_{out} . Thus, the contour evolution equation is corrupted by noise.

Fig. 11(b) shows the results using the cubic spline interpolation method [27]. The smoothness of the contour depends only on the contour length regularization parameter β . However, the foam in the wake of the boat is kept as part of the object.

Fig. 11(c) shows the results using the new smoothing spline method proposed here. The smoothness of the contour depends only on the smoothing spline parameter λ . Relaxing the rigid interpolation constraint brings an obvious improvement: The foam is not kept anymore, whereas the object is still reasonably well segmented.

This third experiment confirms the range of $[0.1, 1]$, we determined, as standard values for the parameter λ .

Fig. 12 shows the computation time and the accuracy of the segmentation on the “coastguard” sequence, for the 5 first images. The contour is sampled with 64 knots and the size of the image is 352×288 . The sequence is segmented with a *Pentium IV at 2.6 GHz*. The initial contour for the first frame is given by the image boundaries. For the frames 2, 3, 4, and 5, the initialization is provided by the final contour in the previous frame. The object in the first frame takes more time to be segmented because the initial contour is “far” from the object. For the other frames, the segmentation is achieved in less than 0.40 s/frame (with a Pentium IV at 2.6 GHz). Thus, the whole segmentation process should be ten times faster to provide results in real time. According to our knowledge, such a factor is not out of reach by optimization for an industry expert.

We can, thus, say that the smoothing spline method provides global robustness to noise-like data. The accuracy results on a real video sequence show the improvement of our smoothing spline method over a direct regularization of the segmentation criterion.

V. CONCLUSION

In this paper, we address the problem of image and video segmentation by working out a new region-based method using cubic smoothing spline active contours.

Instead of spline interpolation, we have chosen a smoothing spline approximation because we want the method to be more

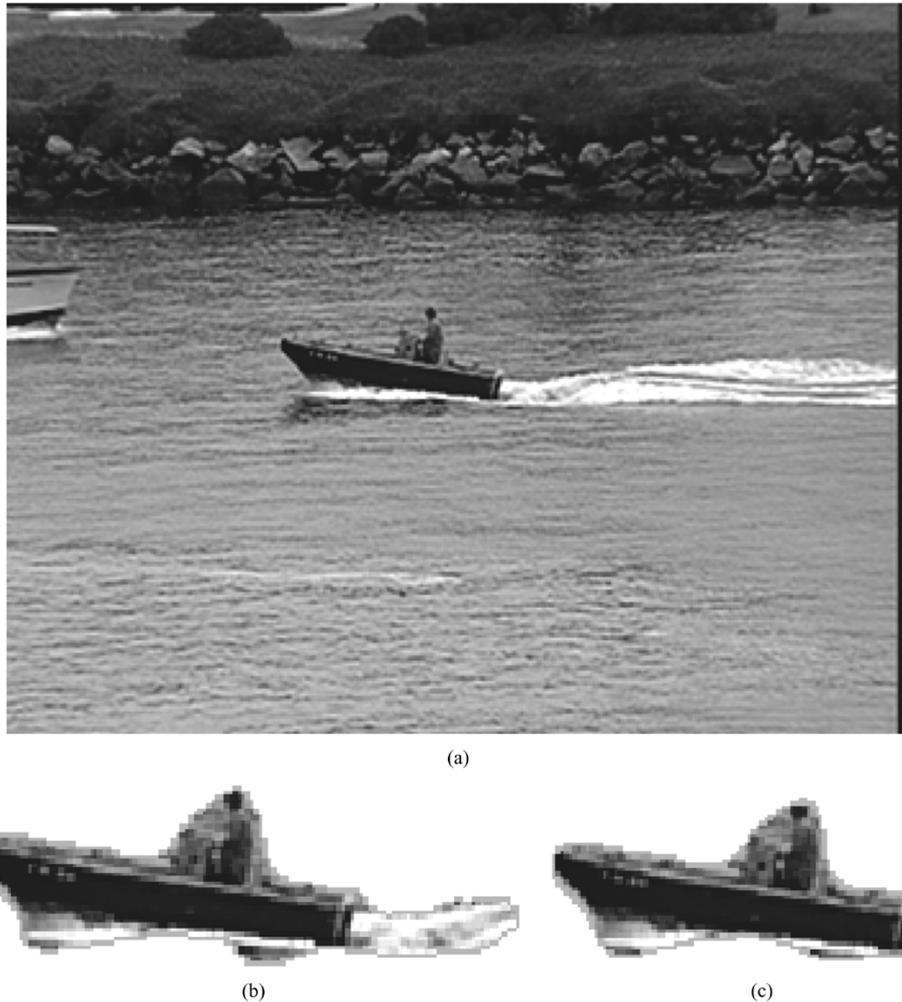


Fig. 11. Smoothing spline to smooth contours. (a) Initial sequence. (b) Interpolation $\lambda = 0$ and $\beta = 20$. (c) Approximation $\lambda = 0.3$ and $\beta = 0$.

robust in the presence of noise. The smoothing spline parameter λ provides a tunable tradeoff between *interpolation error* and *contour smoothness*. Furthermore, increasing the smoothing spline parameter λ improves the sampling uniformity of the contour and avoids the presence of loops. The structure of the contour remains stable to variations of this parameter which is not true with variations of β , the weight on the length penalty. The robustness of the active contour with respect to λ suggested that we could determine a range for standard variations of this parameter. Our experiments provided a range of $[0.1, 1]$. As a consequence of the very low computational cost of the B-spline implementation, real-time segmentation is achieved.

APPENDIX I CUBIC SPLINE INTERPOLATION

A. Recursive Filter Factorization

Assuming that the data points P are uniformly sampled, the interpolating cubic spline filter $(B_1^3(z))^{-1}$, given in (10), can be factorized into a product of causal and anticausal filters [33]

$$(B_1^3(z))^{-1} = \frac{6}{z+4+z^{-1}} = \left(\frac{-6z_1}{1-z_1z} \right) \left(\frac{1}{1-z_1z^{-1}} \right) \quad (26)$$

where $z_1 = -2 + \sqrt{3}$.

This factorization results in a cascade of first-order causal and anticausal recursive filters. Thus, given the data points $\{P(k)\}_{k=0,\dots,N-1}$, the right-hand-side factorization provides the cubic spline interpolating coefficients $\{Q(k)\}_{k=0,\dots,N-1}$ through the following recursive algorithm:

$$\tilde{Q}(k) = z_1\tilde{Q}(k-1) + P(k) \quad (27)$$

$$Q(k) = z_1Q(k+1) - 6z_1\tilde{Q}(k) \quad (28)$$

for all integer k , and where $\tilde{Q}(k)$ are intermediate coefficients. We have to specify the initialization for the two recursions.

B. Initialization

1) *Causal Filtering*: The first recursion (27) leads to the following relation:

$$\begin{aligned} \tilde{Q}(N-k) &= P(N-k) + z_1P(N-k-1) \\ &\quad + z_1^2P(N-k-2) + \dots \\ &\quad + z_1^{N-1}P(N-k-(N-1)) \\ &\quad + z_1^N\tilde{Q}(-k). \end{aligned} \quad (29)$$

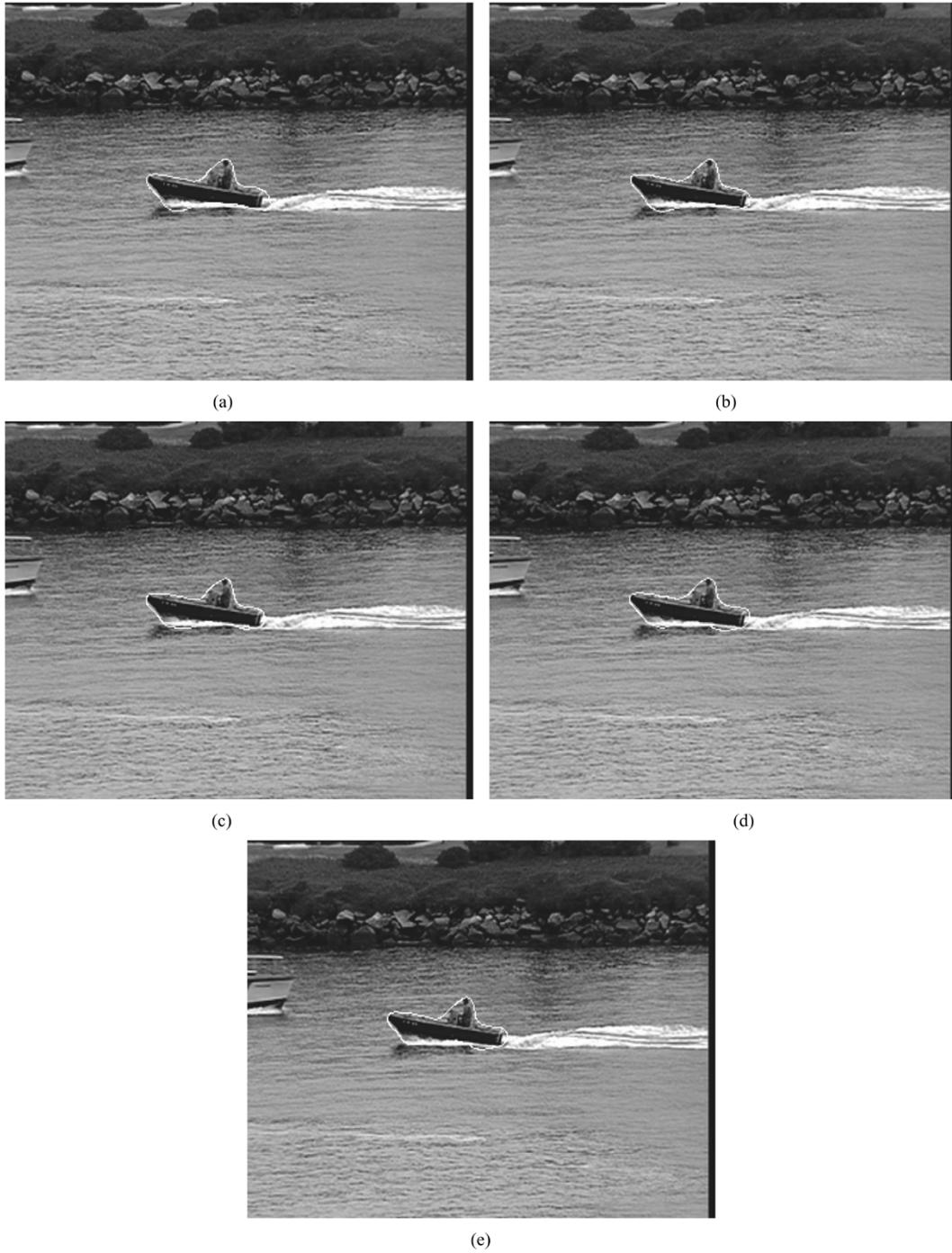


Fig. 12. Computation time of the segmentation. (a) Frame 1: 1.33 s. (b) Frame 2: 0.12 s. (c) Frame 3: 0.30 s. (d) Frame 4: 0.42 s. (e) Frame 5: 0.25 s.

Because the curve is closed, the data points are N periodic, i.e., $P(N - k) = P(-k)$ for all integer k . As a result of the filtering operations, the coefficients $\tilde{Q}(k)$ and $Q(k)$ are N periodic, as well.

Letting $k = 0$ in (29) and using the N periodicity of $\tilde{Q}(k)$ provides $\tilde{Q}(0)$

$$\tilde{Q}(0) = \left(\frac{1}{1 - z_1^N} \right) \sum_{l=0}^{N-1} z_1^l P(N - l). \quad (30)$$

The others coefficients $\tilde{Q}(1), \tilde{Q}(2), \dots, \tilde{Q}(N - 1)$ are obtained by applying the induction (27).

2) *Anticausal Filtering*: We now apply the anticausal filter (28) on the coefficients $\tilde{Q}(k)$ and, in order to trigger the recursion, we need to initialize it by providing the value of $Q(N) = Q(0)$.

Similarly as for the causal case, we obtain the following expression for $Q(0)$:

$$Q(0) = Q(N) = - \left(\frac{6z_1}{1 - z_1^N} \right) \sum_{l=0}^{N-1} z_1^l \tilde{Q}(l). \quad (31)$$

Then, the induction (28) provides $Q(N - 1), Q(N - 2) \dots Q(1)$.

We have, thus, specified the appropriate starting values for both causal and anticausal filtering. We cascade these filters with data points P to compute cubic spline coefficients Q . The recursive algorithm is stable numerically, fast and easy to implement.

APPENDIX II CUBIC SMOOTHING SPLINE APPROXIMATION

A. Recursive Filter Factorization

Assuming that the data points P are uniformly sampled, the smoothing cubic spline filter $(S_\lambda^3(z))^{-1}$, given in (15), can be factorized into a product of causal and anticausal filters.

Let us consider the denominator of $(S_\lambda^3(z))^{-1}$

$$D(z) = z + 4 + z^{-1} + 6\lambda(z^2 - 4z + 6 - 4z^{-1} + z^{-2}). \quad (32)$$

This polynomial can be factorized as

$$\begin{aligned} D(z) &= \frac{6\lambda}{b}(1 + az + bz^2)(1 + az^{-1} + bz^{-2}) \\ &= \frac{6\lambda}{b}S_1(z^{-1})S_1(z) \end{aligned} \quad (33)$$

where a and b are *real* numbers. Moreover, because $D(z)$ does not cancel on the unit circle, $S_1(z)$ has its roots—whether real or complex—strictly inside the unit circle. This shows that the smoothing spline prefilter can be implemented as a cascade of second-order causal and anticausal recursive filters

$$S_\lambda^3(z) = \frac{b}{\lambda} \cdot \frac{1}{1 + az^{-1} + bz^{-2}} \cdot \frac{1}{1 + az + bz^2}. \quad (34)$$

Note that, by defining $x = z - 2 + z^{-1}$, we can rewrite (32) as $D(z) = 6\lambda x^2 + x + 6$ the roots of which are either real, when $\lambda \leq 1/144$, or complex, when $\lambda > 1/144$. This implies that the roots of $S_1(z)$ are either real, when $\lambda \leq 1/144$, or complex, when $\lambda > 1/144$. It is only when $\lambda = 1/144$ that $S_1(z)$ has double roots.

Given the data points $\{P(k)\}_{k=0,\dots,N-1}$, the right-hand-side factorization of (34) leads to the cubic smoothing spline coefficients $\{Q(k)\}_{k=0,\dots,N-1}$ by the following recursive algorithm:

$$\tilde{Q}(k) = -a\tilde{Q}(k-1) - b\tilde{Q}(k-2) + P(k) \quad (35)$$

$$Q(k) = -aQ(k+1) - bQ(k+2) + \frac{b}{\lambda}\tilde{Q}(k). \quad (36)$$

We now have to specify the appropriate initialization for the two recursions.

B. Initialization

In order to determine the initialization of the recursive filtering algorithm, we need to compute the impulse response $s_1(n)$ of the causal filter $S_1(z)^{-1}$ in the cascade expression (34).

- When $\lambda = 1/144$, $S_1(z) = (1 - z_0 z^{-1})^2$ with $z_0 = -5 + 2\sqrt{6}$ and we immediately have

$$\frac{1}{S_1(z)} = \sum_{n \geq 0} (n+1)z_0^n z^{-n}$$

from which we obtain

$$s_1(n) = (n+1)z_0^n u(n)$$

where $u(n)$ is the discrete step sequence $u(n) = 1$ for $n \geq 0$ and $u(n) = 0$ otherwise.

- When $\lambda \neq 1/144$, the two roots z_0 and z_1 of $S_1(z)$ are distinct. We can, thus, decompose $S_1(z)^{-1}$ in simple fractions

$$\frac{1}{S_1(z)} = \frac{A}{1 - z_0 z^{-1}} + \frac{B}{1 - z_1 z^{-1}}$$

where $A = (1 - z_1 z_0^{-1})^{-1}$ and $B = (1 - z_0 z_1^{-1})^{-1}$. As a result, the impulse response of $S_1(z)^{-1}$ is given by

$$s_1(n) = Az_0^n u(n) + Bz_1^n u(n).$$

Note that the impulse response of the anticausal filter $S_1(z^{-1})^{-1}$ (needed for the initialization of the anticausal recursion) is given by $s_1(-n)$.

1) *Causal Recursion:* The initialization of (35) requires computing $\tilde{Q}(0)$ and $\tilde{Q}(1)$. Using the impulse response of $S_1(z)^{-1}$, we have

$$\tilde{Q}(0) = \sum_{n \in \mathbb{Z}} s_1(-n)P(n)$$

$$\tilde{Q}(1) = \sum_{n \in \mathbb{Z}} s_1(1-n)P(n)$$

then, using the N periodicity of $P(n)$ (closed contour)

$$\tilde{Q}(0) = \sum_{n_0=0}^{N-1} P(n_0) \sum_{n \in \mathbb{Z}} s_1(-n_0 + nN)$$

$$\tilde{Q}(1) = \sum_{n_0=0}^{N-1} P(n_0) \sum_{n \in \mathbb{Z}} s_1(1 - n_0 + nN). \quad (37)$$

We, thus, need to compute an expression of the form $\sum_n s_1(k + nN)$. For this, we consider the functions

$$g_k(r) = \sum_{n \in \mathbb{Z}} r^{k+nN} u(k + nN) \text{ with } |r| < 1.$$

Since $g_k(r)$ obviously satisfies $g_k(r) = g_{k+N}(r)$, we can restrict k to $[0, N-1]$ and we find

$$g_k(r) = \sum_{n \geq 0} r^{k+nN} = \frac{r^k}{1 - r^N}.$$

Thanks to the N periodicity, k has to be replaced by $(k \bmod N)$ in this expression when $k \notin [0, N-1]$. Moreover, by simple differentiation of $g_{k+1}(r)$, we also have that

$$\begin{aligned} \sum_{n \in \mathbb{Z}} (k + nN + 1)r^{k+nN} u(k + nN) \\ = g'_{k+1}(r) = \frac{(k+1)r^k}{1 - r^N} + \frac{Nr^{N+k}}{(1 - r^N)^2}. \end{aligned} \quad (38)$$

Finally, we find that

- when $\lambda = 1/144$

$$\sum_{n \in \mathbb{Z}} s_1(k + nN) = g'_{(k \bmod N)+1}(z_0); \quad (39)$$

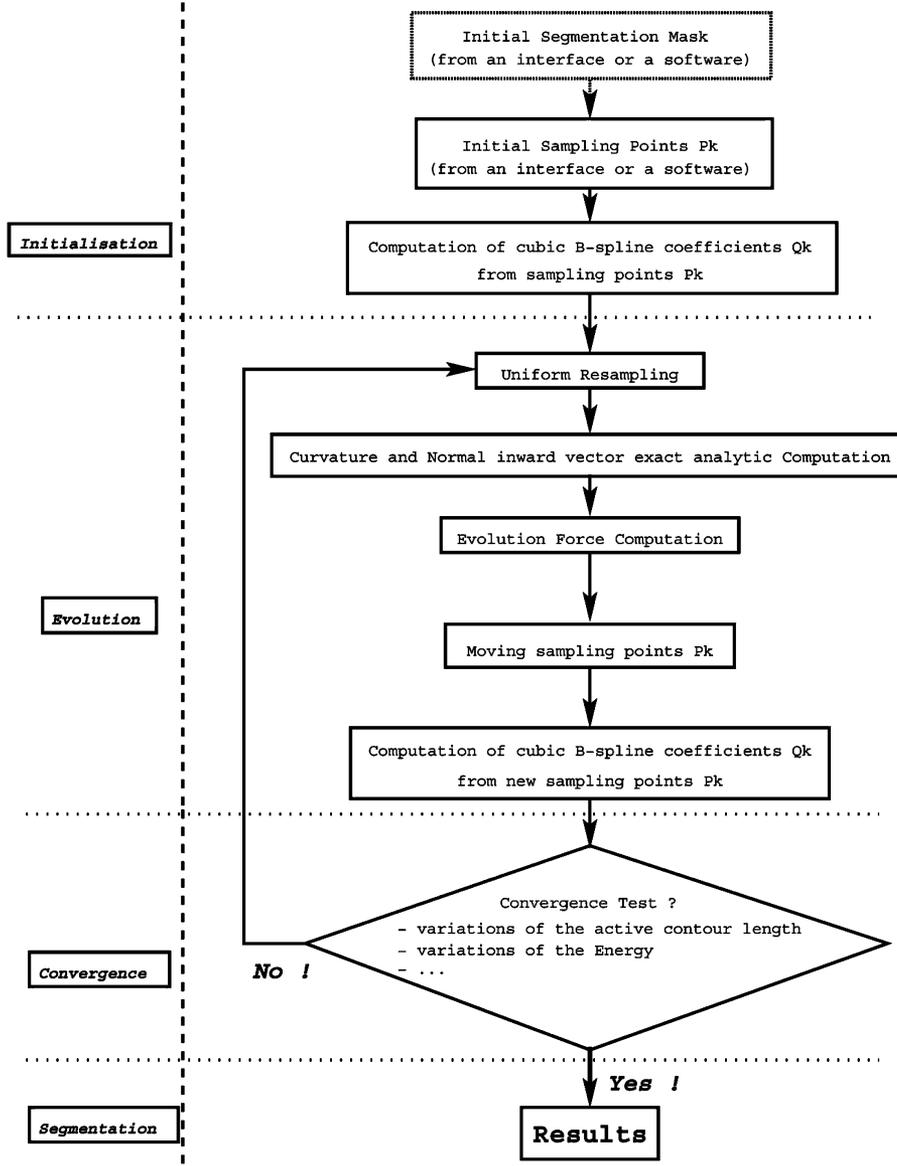


Fig. 13. Flow-chart of our algorithm based on cubic spline interpolation.

- when $\lambda \neq 1/144$

$$\sum_{n \in \mathbb{Z}} s_1(k + nN) = Ag_{k \bmod N}(z_0) + Bg_{k \bmod N}(z_1). \quad (40)$$

These expressions can be substituted in (37) to provide the initial conditions to the recursion (35).

2) *Anticausal Recursion:* The initialization of (36) requires computing $Q(N-1)$ and $Q(N-2)$. Using the impulse response $s_1(-n)$ of $S_1(z^{-1})^{-1}$, we obtain

$$Q(N-1) = \frac{b}{\lambda} \sum_{n \in \mathbb{Z}} s_1(-(N-1-n)) \tilde{Q}(n)$$

$$Q(N-2) = \frac{b}{\lambda} \sum_{n \in \mathbb{Z}} s_1(-(N-2-n)) \tilde{Q}(n)$$

then, using the N periodicity of $\tilde{Q}(n)$ (closed contour)

$$Q(N-1) = \frac{b}{\lambda} \sum_{n_0=0}^{N-1} \tilde{Q}(n_0) \sum_{n \in \mathbb{Z}} s_1(n_0 + 1 + nN)$$

$$Q(N-2) = \frac{b}{\lambda} \sum_{n_0=0}^{N-1} \tilde{Q}(n_0) \sum_{n \in \mathbb{Z}} s_1(n_0 + 2 + nN). \quad (41)$$

By substituting the expressions found in (39) and (40) in these equations, (41) provides the initial conditions to the recursion (36).

To summarize the process described above, given data points $\{P(n)\}_{n=0 \dots N-1}$, we cascade a causal and an anticausal filter to compute the cubic smoothing spline coefficients $\{Q(n)\}_{n=0 \dots N-1}$. As for interpolating spline, the recursive algorithm for smoothing spline is stable numerically, fast, and easy to implement.

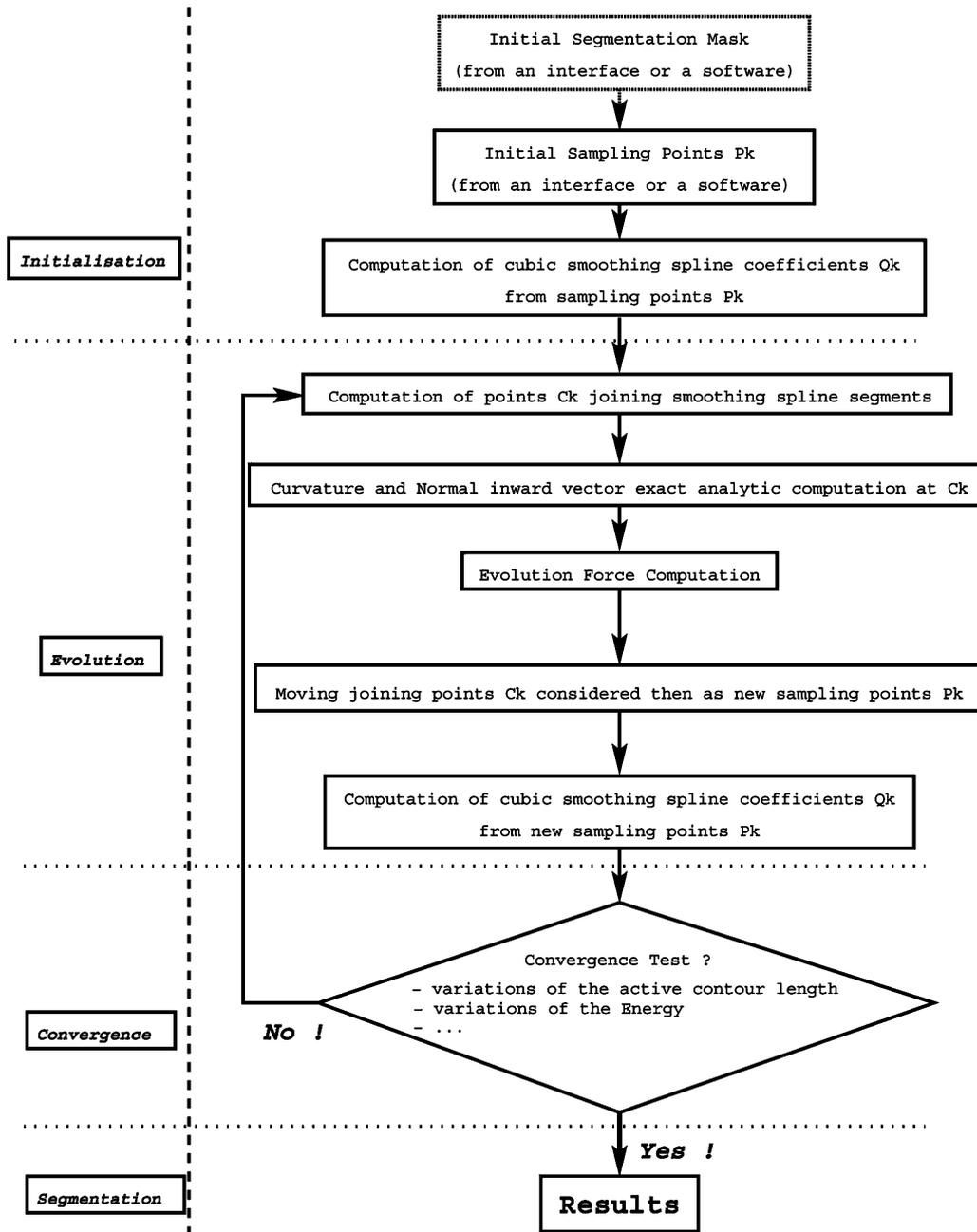


Fig. 14. Flow-chart of our algorithm based on smoothing spline approximation.

APPENDIX III FLOW-CHARTS OF THE ALGORITHMS

A. Cubic Spline Interpolation

See Fig. 13.

B. Cubic Smoothing Spline Approximation

See Fig. 14.

ACKNOWLEDGMENT

The authors would like to thank A. Herbulot, Ph.D. student at I3S Lab, for her helpful contribution to the section on segmen-

tation of homogeneous regions in color video sequences. They would also like to thank DMS for providing osteoprosis images.

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