A NEW HIGH-RESOLUTION PROCESSING METHOD FOR THE DECONVOLUTION OF OPTICAL COHERENCE TOMOGRAPHY SIGNALS

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ABSTRACT

We show the feasibility and the potential of a new signal processing algorithm for the high-resolution deconvolution of OCT signals.

Our technique relies on the description of the measures in a parametric form, each set of four parameters describing the optical characteristics of a physical interface (e.g., complex refractive index, depth). Under the hypothesis of a Gaussian source light, we show that it is possible to recover the 4K parameters corresponding to K interfaces using as few as 4K uniform samples of the OCT signal. With noisy data, we can expect the robustness of our method to increase with the oversampling rate—or with the redundancy of the measures.

The validation results show that the quality of the estimation of the parameters (in particular the depth of the interfaces) is narrowly linked to the noise level of the OCT measures—and not to the coherence length of the source light—and to their degree of redundancy.

1 INTRODUCTION

Optical Coherence Tomography (OCT) is a recent high-resolution imaging technique [1, 2, 3]. It is based on an interferometric measure in which a wave with low temporal coherence is split into two parts. One of the beams hits the object to image, is backscattered and guided to a photocaptor, while the second one acts as a reference and is guided to the photocaptor as well, where it is recombined with the object wave to yield interferences. Varying the pathlength of the reference wave, one is able to scan inside the object at depths such that the backscattered wave keeps some coherence with the incident one (see Fig. 1).

The OCT signal essentially carries the information of abrupt changes in the refractive index and the depth-resolution that can be attained is roughly half the coherence length of the reference wave [4]. In common experiments, this resolution is between 4μ m and 16μ m [5], although using a Fourier deconvolution technique might improve this figure [6]

We propose here a direct signal processing method that is able to reach a resolution that does not depend on the coherence length, but rather on the noise level of the OCT measure. This highresolution parametric method is reminiscent of the retrieval of complex exponentials in a noisy signal, which is a standard signal pro-



Fig. 1. Schematical overview of an OCT measure. The object is reduced to its interfaces as in the model used for this paper (see Section 2.2).

cessing problem, e.g., in mobile communications [7]. Our technique is actually exact under the assumption of a Gaussian coherence function; it is also "critical" in the absence of noise—the retrieval of N parameters requires no more than N samples of the interference pattern. The redundancy in the OCT measure, which may be quite high, can thus be exploited to reduce noise.

2 MODELIZATION OF THE OCT SIGNAL

2.1 Standard Convolution Model

An incident 1D complex wave $\psi(t - x/c)$, whose coherence function (and power spectrum density $S(\nu) = \hat{G}(\nu)$) is defined by

$$G(t_2 - t_1) = \langle \psi(t_1)^* \psi(t_2) \rangle \tag{1}$$

illuminates an object that we want to image. We assume that this object is characterized by a linear time-invariant impulse response h(t), which implies that it is the source of a backpropagating reflected wave $\psi_{\rm R}(t+x/c)$, where $\psi_{\rm R} = h * \psi$. This wave is guided to the photocaptor along a path of parameterized (variable) length x_1 . The incident wave is also guided to this photocaptor along a path of (fixed) length x_0 and the average intensity resulting from

the superposition of the two waves is measured

$$I(x_1 - x_0) = \left\langle \left| \psi\left(t + \frac{x_0}{c}\right) + \psi_{\mathrm{R}}\left(t + \frac{x_1}{c}\right) \right|^2 \right\rangle$$
$$= \int \left| 1 + \hat{h}(\nu) e^{2i\pi\nu \frac{x_1 - x_0}{c}} \right|^2 S(\nu) \,\mathrm{d}\nu$$
$$= \operatorname{const} + 2\mathscr{R} \left\{ h * G\left(\frac{x_1 - x_0}{c}\right) \right\}.$$

Finally, the signal that has to be processed is

$$I_0(x) = 2\mathscr{R}\left\{h * G(\frac{x}{c})\right\}$$
(2)

We assume here that the power spectrum density of the incident light is Gaussian

$$S(\nu) = \frac{1}{\sqrt{2\pi}\Delta\nu} e^{-\frac{1}{2}\left(\frac{\nu-\nu_0}{\Delta\nu}\right)^2}$$

$$\stackrel{\uparrow}{\Rightarrow} \mathcal{F}$$

$$G(t) = e^{-\frac{(2\pi\Delta\nu)^2}{2}t^2 + 2i\pi\nu_0 t}$$
(3)

where ν_0 is the central frequency of the source and $\Delta \nu$ is related to its temporal coherence length, l_c , through $l_c = \frac{\sqrt{2 \log 2}}{\pi} \frac{c}{\Delta \nu}$ [4].

2.2 Multilayer Parametric Model

As can be seen from (2) and (3), the OCT signal is a bandpass version of the signature h(t) of the object. In particular, this means that attempting to reconstruct the low-pass portion of h(t) from the OCT measurements, $I_0(t)$, is an ill-posed problem. This implies that it is only the transitional features of the object that are likely to be extracted, because they alone have a sufficiently large bandwidth to intersect the support of $S(\nu)$.

This is why we propose to model the object as a succession of interfaces between which the refractive index is constant. To simplify even more, we consider here the unidimensional case characterized by a complex refractive index

$$n(x) = \begin{cases} n_0 \text{ for } x < x_1 \\ n_k \text{ for } x_k \le x < x_{k+1} \text{ and } k = 1 \dots K - 1 \\ n_K \text{ for } x_K \le x \end{cases}$$

and by the wave equation $y''(x) + \left(\frac{2\pi\nu}{c}\right)^2 n(x)^2 y(x) = 0$. Then, the Fourier transform of the impulse response h(t) is

Then, the Fourier transform of the impulse response h(t) is given by

$$\hat{h}(\nu) = \sum_{k=1}^{K} a_k e^{-2i\pi b_k \nu/c} \quad \text{for all } |\nu - \nu_0| \le \frac{\Delta \nu}{2}, \quad (4)$$

neglecting multiple reflections. Here, a careful analysis of the wave equation provides the relation between (a_k, b_k) and (x_k, n_k) .

As a consequence, the OCT signal can be parameterized as a sum of Gabor functions

$$I_0(x) = 2 \mathscr{R} \left\{ \sum_{k=1}^K \alpha_k e^{-\frac{1}{2\sigma^2} (x - \beta_k)^2} \right\}$$
(5)

where $\alpha_k = a_k e^{-\frac{\nu_0^2}{2\Delta\nu^2}}$, $\beta_k = b_k + i\frac{\nu_0 c}{2\pi\Delta\nu^2}$ and $\sigma = \frac{l_c}{2\sqrt{2\log 2}}$. The purpose of this paper is to present an *exact* method for identifying the parameters α_k and β_k from a *finite number* of samples of $I_0(x)$.

3 A HIGH-RESOLUTION METHOD

We will from now on assume that we know the value of l_c , and hence, of σ . Moreover, we have access to the measurements $J_l = I_0(l\Delta x)$ for $l = l_0 \dots l_1$ where Δx is a sampling step. Thus, we have

$$J_l = 2 \mathscr{R} \left\{ \sum_{k=1}^{K} \alpha_k e^{-\frac{\Delta x^2}{2\sigma^2} \left(l - \frac{\beta_k}{\Delta x} \right)^2} \right\}.$$
 (6)

Multiplying left and right hand sides by $e^{\frac{\Delta x^2}{2\sigma^2}(l-m)^2}$ yields

$$y_{l} = e^{\frac{\Delta x^{2}}{2\sigma^{2}}(l-m)^{2}}J_{l}$$

$$= 2\mathscr{R}\left\{\sum_{k=1}^{K}\alpha_{k}e^{\frac{\Delta x^{2}}{2\sigma^{2}}\left(\frac{\beta}{\Delta x}-m\right)\left(2l-m-\frac{\beta}{\Delta x}\right)}\right\}$$

$$= \sum_{k=1}^{K}\alpha_{k}'z_{k}^{l} + \sum_{k=1}^{K}\alpha_{k}'^{*}(z_{k}^{*})^{l}$$
(7)

where we have defined $\alpha'_{k} = \alpha_{k} e^{-\frac{\Delta x^{2}}{2\sigma^{2}} \left(\frac{\beta}{\Delta x} - m\right) \left(m + \frac{\beta}{\Delta x}\right)}$ and

 $z_k = e^{\frac{\Delta x^2}{\sigma^2} \left(\frac{\beta}{\Delta x} - m\right)}$. The advantage of the last expression is that it takes a standard form that can be analyzed using a high-resolution method [7].

3.1 Finding the z_k and α'_k

Let P(z) be the real polynomial that has the roots z_k, z_k^*

$$P(z) = \prod_{k=1}^{K} (z - z_k)(z - z_k^*) = \sum_{k=0}^{2K} p_k z^k.$$

One can then easily verify that

$$\forall l = l_0 + 2K, \dots, l_1, \quad \sum_{k=0}^{2K} p_k y_{l-k} = 0.$$

These linear equations are now written in a matrix form

$$\underbrace{\begin{pmatrix} y_{l_0+2K} & y_{l_0+2K-1} & \dots & y_{l_0} \\ y_{l_0+2K+1} & y_{l_0+2K} & \dots & y_{l_0+1} \\ y_{l_0+2K+2} & y_{l_0+2K+1} & \dots & y_{l_0+2} \\ \vdots & \vdots & \vdots & \vdots \\ y_{l_1} & y_{l_1-1} & \dots & y_{l_1-2K} \end{pmatrix} \begin{pmatrix} p_0 \\ p_1 \\ p_2 \\ \vdots \\ p_{2K} \\ p_{2K} \end{pmatrix}}_{\mathbf{P}} = 0,$$

where, **A** is a matrix having $(l_1 - l_0 - 2K + 1)$ lines and (2K+1) columns. In particular, we see that, with as few as 4K samples, we are able to reconstruct the polynomial P(z). Extracting its roots provides the unknown values z_k .

Then, the parameters α'_k are obtained by solving the linear Vandermonde system of equations obtained from (7)

$$\begin{pmatrix} z_1^{l_0} & z_1^{*l_0} & \dots & z_K^{l_0} & z_K^{*l_0} \\ z_1^{l_0+1} & z_1^{*l_0+1} & \dots & z_K^{l_0+1} & z_K^{*l_0+1} \\ \vdots & \vdots & \vdots & \vdots & \vdots \\ z_1^{l_1} & z_1^{*l_1} & \dots & z_K^{l_1} & z_K^{*l_1} \end{pmatrix} \begin{pmatrix} \alpha_1' \\ \alpha_1'' \\ \vdots \\ \alpha_K' \\ \alpha_K'' \end{pmatrix} = \begin{pmatrix} y_{l_0} \\ y_{l_0+1} \\ \vdots \\ y_{l_1} \end{pmatrix}.$$

In order to find the values α'_k , we need no fewer than 2K measures J_l . On the whole, we conclude that we are able to reconstruct uniquely the 2K complex-valued parameters (α'_k, z_k) as soon as we are provided with 4K real-valued uniform measures J_l . In the next subsection, we will see how it is possible to exploit the redundancy of these measures when they are corrupted by noise.

3.2 The Noisy case

Usually, the data are noisy and/or the model does not fit the data exactly. In this case, we propose first to enhance the signal, and then to solve the two linear systems of equations above in the least-square sense—in practice, this involves finding the smallest eigenvalue of the matrix $\mathbf{A}^{T}\mathbf{A}$.

Our denoising technique uses the information that y_n has the parametric form (7). In the absence of noise, the matrix

$$\mathbf{B}_{N} = \begin{pmatrix} y_{l_{0}+N} & y_{l_{0}+N-1} & \dots & y_{l_{0}} \\ y_{l_{0}+N+1} & y_{l_{0}+N} & \dots & y_{l_{0}+1} \\ y_{l_{0}+N+2} & y_{l_{0}+N+1} & \dots & y_{l_{0}+2} \\ \vdots & \vdots & \vdots & \vdots \\ y_{l_{1}} & y_{l_{1}-1} & \dots & y_{l_{1}-N} \end{pmatrix}$$

is always of rank 2K when $N \ge 2K$. Its decomposition in singular values $\mathbf{B}_N = \mathbf{Q} \mathbf{\Delta} \mathbf{R}^T$ therefore involves a diagonal matrix $\mathbf{\Delta}$ with only 2K nonzero values. Our direct denoising method can now be described as follows:

- First, choose a denoising length N. The longer it is, the larger the reduction of the noise—but also, the more computationally expensive it is.
- Second, perform the decomposition of the noisy measurement matrix B_N in singular values.
- Third, build the "denoised" diagonal matrix by keeping only the 2K largest coefficients of Δ; then reconstruct the denoised measurement matrix B̂_N = QÂR^T.
- Last, since every column of B_N provides an estimate of the signal, build a denoised version of the signal by averaging over the estimates of y_l obtained from the N + 1 columns of B_N.

This denoising technique has proved extremely efficient on the test signals that we have analyzed. For instance, with 350 samples, two Gaussians to retrieve, and a denoising length of N = 50, the signal to noise ratio increase usually exceeds 16 dB.

4 VALIDATION RESULTS

We have synthetized 353 uniform samples of an OCT signal simulating the reflection of two interfaces separated by a distance of 2.66 μ m and inducing a wavelength shift from 1300 nm to 1302 nm and 1339 nm, respectively. The coherence length for the Gaussian source is 20 μ m, so the equivalent depth resolution is 10 μ m. We have added a Gaussian white noise ranging from 6 dB to 60 dB and have applied our algorithm to these 353 samples. An instance of this noisy simulated OCT signal is shown in Fig. 2.

The main retrieved parameters (position and frequency) are shown in the scatterplots of Figs. 3 and 4. Using these estimated parameters we reconstructed a signal that is much closer to the original noise-free signal than to the noisy one. More precisely, our reconstruction increases the signal to noise ratio by 16 dB on average as shown in Fig. 5. This gain is identical to $\sqrt{\text{redundancy}}$ which is what we would expect from an optimal estimator.



Fig. 2. Simulated OCT signal—Gaussian light source at 1300 nm with 20 μ m temporal coherence length—composed of two modulated Gaussians and corrupted with 20 dB noise. Here, the "standard" axial resolution is 20 μ m/2 = 10 μ m.

5 CONCLUSION

We have presented a new high-resolution signal processing method for the deconvolution of OCT signals. In particular, we have shown that the resolution of our method is only limited by the amount of noise that is present in the measures: less noisy data yield higher resolved structures. Moreover, our technique is versatile as it requires only a finite number of samples for the exact retrieval of the parameters that describe the OCT signal. It may be used either when few but noise-free data are available, or in the case of oversampled noisy measurements.

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Fig. 3. Positions of the interfaces as a function of the input noise. Notice that the depth resolution depends only on the noise level, not on the coherence length which is here a constant.



Fig. 4. Retrieved wavelengths as a function of the input noise. Observe that the frequency resolution does not depend on the coherence length—nor, actually, on the length of the signal.



Fig. 5. Error between the original signal and the reconstruction using the retrieved noisy parameters (in ordinate) as a function of the level of input noise (in abscissa). To ease the comparison, we have drawn the y = x line. Note that the level of output noise is reduced dramatically (16 dB on average) which shows the efficiency of our method in exploiting the redundancy of the measures.